

Research article

## Oxygen uptake kinetics during incremental- and decremental-ramp cycle ergometry

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### Abstract

The pulmonary oxygen uptake ( $\text{VO}_2$ ) response to incremental-ramp cycle ergometry typically demonstrates lagged-linear first-order kinetics with a slope of  $\sim 10\text{-}11 \text{ ml}\cdot\text{min}^{-1}\cdot\text{W}^{-1}$ , both above and below the lactate threshold ( $\theta_L$ ), i.e. there is no discernible  $\text{VO}_2$  slow component (or “excess”  $\text{VO}_2$ ) above  $\theta_L$ . We were interested in determining whether a reverse ramp profile would yield the same response dynamics. Ten healthy males performed a maximum incremental -ramp ( $15\text{-}30 \text{ W}\cdot\text{min}^{-1}$ , depending on fitness). On another day, the work rate (WR) was increased abruptly to the incremental maximum and then decremented at the same rate of  $15\text{-}30 \text{ W}\cdot\text{min}^{-1}$  (step-decremental ramp). Five subjects also performed a sub-maximal ramp-decremental test from 90% of  $\theta_L$ .  $\text{VO}_2$  was determined breath-by-breath from continuous monitoring of respired volumes (turbine) and gas concentrations (mass spectrometer). The incremental-ramp  $\text{VO}_2$ -WR slope was  $10.3 \pm 0.7 \text{ ml}\cdot\text{min}^{-1}\cdot\text{W}^{-1}$ , whereas that of the descending limb of the decremental ramp was  $14.2 \pm 1.1 \text{ ml}\cdot\text{min}^{-1}\cdot\text{W}^{-1}$  ( $p < 0.005$ ). The sub-maximal decremental-ramp slope, however, was only  $9.8 \pm 0.9 \text{ ml}\cdot\text{min}^{-1}\cdot\text{W}^{-1}$ : not significantly different from that of the incremental-ramp. This suggests that the  $\text{VO}_2$  response in the supra- $\theta_L$  domain of incremental-ramp exercise manifest not actual, but pseudo, first-order kinetics.

**Key words:** Oxygen uptake-work rate gain, incremental-ramp exercise, decremental-ramp exercise, system linearity.

### Introduction

The magnitude and profile of the pulmonary oxygen uptake ( $\text{VO}_2$ ) response during incremental-ramp cycle ergometry are widely used as characteristics of the determinants of exercise tolerance in humans, i.e. its gain ( $\Delta\text{VO}_2/\Delta\text{WR}$ ), response time constant and its maximum (e.g. Whipp et al., 1981). Typically, at all but extremely slow incrementation rates (Hansen et al., 1988; Whipp and Mahler 1980; Zoladz et al. 1995), the  $\text{VO}_2$  response to such tests demonstrates the lagged-linear behaviour characteristic of first-order kinetics, with the  $\text{VO}_2$  ‘lag’, relative to steady-state  $\text{VO}_2$  requirement for that work rate (WR), reflecting the mean response time (MRT) for the kinetics (Linnarsson, 1974; Hughson and Morrissey, 1982), as schematised in Figure 1a.

The gain of the  $\text{VO}_2$  response during incremental-ramp exercise has been shown not to differ significantly from that of its steady-state  $\text{O}_2$  cost for cycle ergometry (Whipp et al., 1981), with values of  $\sim 9\text{-}11 \text{ ml}\cdot\text{min}^{-1}\cdot\text{W}^{-1}$

(e.g. Davis et al., 1982; Hansen et al., 1984; Neder et al., 1999; Whipp et al., 1981), thereby allowing work efficiency to be estimated. While this is the expected  $\text{VO}_2$  profile for a system expressing linear first-order kinetics, it is surprising that this lagged-linear response is conserved during exercise above  $\theta_L$  where, at least for constant-WR exercise,  $\text{VO}_2$  is known to diverge from dynamic system linearity (Hughson and Inman, 1986; Jones and Poole, 2005; Whipp et al., 1981; Yano et al., 2003).

These features of the incremental-ramp  $\text{VO}_2$  profile might suggest that, in response to a symmetrical mirror-image ramp WR profile (i.e. a step-decremental ramp), a similarly-apparent first-order  $\text{VO}_2$  kinetic response would result, as schematised in Figure 1b. However, we had noticed (Whipp et al., 1992) that when we imposed such a mirror-image ramp WR profile, the  $\text{VO}_2$  response was not that implicit from the incremental-ramp behaviour. Rather, the slope of the decremental-ramp  $\text{VO}_2$  response was appreciably greater.

Yano et al. (2004) demonstrated, from a detailed series of studies, that the group-mean  $\text{VO}_2$  slope response of their subjects to decremental-ramp exercise, imposed from a particular absolute high-intensity constant-WR background, was also significantly greater than that in response to incremental exercise of the same WR profile - but of reverse sign. This differed from our previous study (Whipp et al., 1992), in that we utilized the entire incremental tolerance limit and with its mirror-image profile not imposed on a control period with a developing slow phase of the  $\text{VO}_2$  kinetics ( $\text{VO}_{2sc}$ ).

We were therefore interested both in determining whether the different features of the  $\text{VO}_2$  responses to incremental and decremental WR ramps is a consistent feature in individual subjects over the entire tolerance range and what further insights such differences might provide with respect to the control mechanisms for the kinetics of  $\text{VO}_2$  during high-intensity exercise.

### Methods

#### Subjects and procedures

Ten healthy, recreationally-active male volunteers (age  $31 \pm 12$  yr; weight  $71 \pm 8$  kg; height  $1.77 \pm 0.08$  m; peak  $\text{VO}_2$  ( $\text{VO}_{2\text{peak}}$ )  $3.56 \pm 0.59 \text{ l}\cdot\text{min}^{-1}$ ) participated in the study, with each having provided written informed consent. The investigation was approved by the St. George's Hospital Research Ethics Committee, with procedures being con-

ducted in accordance with the Declaration of Helsinki. Prior to testing, the subjects were familiarised with the equipment, procedures and laboratory personnel and, for the 24 hr prior to each testing session, were requested to refrain from participating in strenuous exercise.

### Equipment

The tests were performed on a computer-controlled, electromagnetically-braked cycle ergometer with WR being independent of cycling cadence (Excalibur Sport, Lode, NL). The subjects breathed through a mouthpiece connected to a low-dead space (90 ml), low resistance ( $<1.5$  cm H<sub>2</sub>O at  $3 \text{ L}\cdot\text{s}^{-1}$ ) turbine volume transducer (Interface Associates, Irvine, CA, USA) for the measurement of inspiratory and expiratory airflow and volume; calibration was performed manually with a 3 L syringe (Hans Rudolph, Kansas City, MO, USA) using flow profiles that spanned the experimental range. Respirated gas was continuously sampled at  $1 \text{ ml}\cdot\text{s}^{-1}$  from the mouthpiece and analysed by a quadrupole mass spectrometer (QP9000, Morgan Medical, Gillingham, UK) for [O<sub>2</sub>], [CO<sub>2</sub>] and [N<sub>2</sub>]; calibration was performed using two precision-analysed gas mixtures that spanned the inspiratory-expiratory concentration range. Immediately after each test, the calibration gas mixtures were re-sampled to verify the stability of the calibration. The time delay between the volume and gas concentration signals was measured by passing a bolus of high-CO<sub>2</sub>, low-O<sub>2</sub> gas through the system using a solenoid valve (Beaver et al., 1973) which was then used to phase-align the signals. Following analogue-to-digital conversion, the electrical signals from these devices were sampled and digitised every 20 ms by computer for breath-by-breath determination of ventilatory and gas exchange variables using the algorithms of Beaver et al. and Jenkins et al. (Beaver et al., 1973; Jenkins et al., 1989). The calibration and validation procedures have been described previously (Beaver et al., 1981). Throughout each test, arterial O<sub>2</sub> saturation and heart rate were measured using pulse oximetry (Biox 3745, Ohmeda, Louisville, USA) and the R-R interval of the electrocardiogram (Quest, Burdick, Washington, USA), respectively.

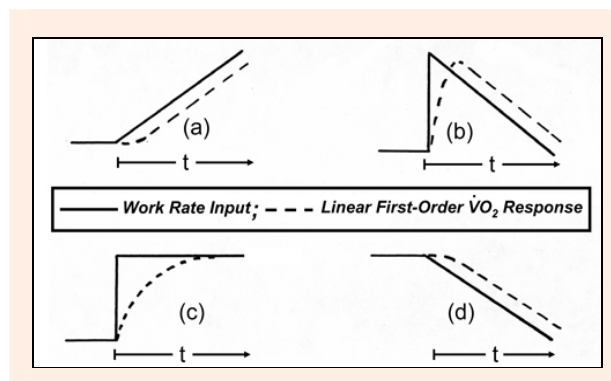
### Exercise protocols

Exercise tests in a given subject were performed on different days. All tests were preceded ( $\geq 4$  min) and followed ( $\geq 6$  min) by a 20 W baseline.

**Incremental-ramp test.** Subjects first completed an incremental-ramp test (Figure 1a;  $15\text{-}30 \text{ W}\cdot\text{min}^{-1}$ ; the chosen WR incrementation rate depending on subject fitness) to the limit of tolerance for: (a) determination of  $\text{VO}_{2\text{peak}}$ , taken to be the mean  $\text{VO}_2$  for an integral number of breaths over the final 20 s of the incremental phase; (b) non-invasive estimation of the lactate threshold ( $\theta_L$ ), using standard ventilatory and gas-exchange criteria (Beaver et al., 1986; Whipp et al., 1986); and (c) the  $\text{VO}_2$ -WR profile.

**Decremental-ramp test.** A maximal decremental-ramp test (Figure 1b) was conducted to allow comparison of the  $\text{VO}_2$ -WR profile with that for the incremental-ramp test. This was a mirror image of the incremental-ramp test: i.e. after an initial 20W baseline phase, the WR was

increased abruptly to the maximum attained on the incremental-ramp test ( $\text{WR}_{\text{max}}$ ) and then decremented back to the 20W baseline at the same rate as that of the incremental-ramp test (i.e.  $15\text{-}30 \text{ W}\cdot\text{min}^{-1}$ ). A subgroup of the subjects ( $n = 5$ ) also completed a sub-maximal decremental-ramp test (Figure 1b), which resembled the maximal decremental-ramp test, except that the WR was initially increased only to 90% of  $\theta_L$  before being decremented back to 20W at the appropriate individual slope of  $15\text{-}30 \text{ W}\cdot\text{min}^{-1}$ . This allowed comparison of the  $\text{VO}_2$ -WR profile with that of both incremental-ramp and the maximal decremental-ramp tests.



**Figure 1.** Schematic representation of linear first-order O<sub>2</sub> uptake ( $\text{VO}_2$ ) responses as a function of time (---) for (a) an incremental ramp exercise test, (b) a step-decremental ramp exercise test, (c) a step (or constant work-rate) exercise test and (d) a decremental ramp exercise test. The work rate profiles are shown as solid lines. See text for further detail.

**Constant-WR test.** The subjects also completed at least three sub- $\theta_L$  constant-WR tests (Figure 1c; as determined from the incremental-ramp test), from a 20W baseline, each of 6 min duration, in order to establish the steady-state  $\text{VO}_2$ -WR relationship.

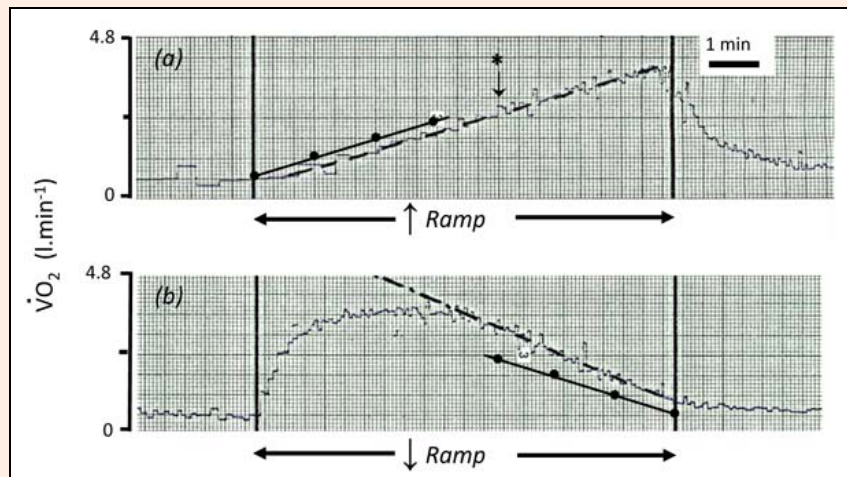
### Data analysis and statistics

The breath-by-breath  $\text{VO}_2$  data were edited to eliminate occasional breaths triggered by, for example, swallows, coughs or sighs which were considered to be uncharacteristic of the underlying physiological response; only breaths  $> 4$  SD of the local mean being excluded (Lamarra et al., 1987). The baseline  $\text{VO}_2$  was taken as the mean  $\text{VO}_2$  for an integral number of breaths over the last 60 s of the 20 W baseline. The slope of the linear phase of the  $\text{VO}_2$ -WR response for incremental-ramp and decremental-ramp tests was obtained by least-squares regression analysis (Origin, Microcal, USA).

A Student's  $t$ -test was used to compare the slopes of the  $\text{VO}_2$ -WR regression lines across the different test types. Differences were considered significant if  $p < 0.05$ . The dispersion about the mean is expressed as  $\pm$  standard deviation (SD), unless otherwise specified.

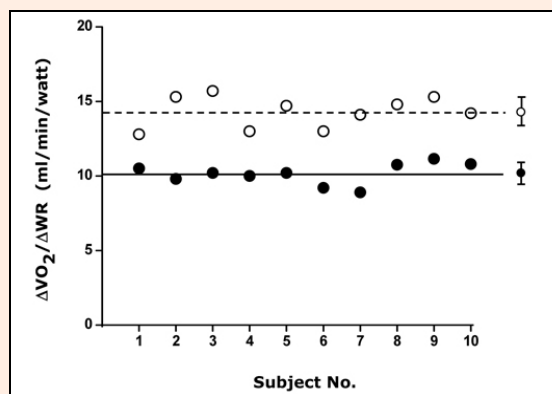
### Results

A representative example of the  $\text{VO}_2$  response profile for the incremental-ramp test is shown in Figure 2a, with the dashed line indicating the response slope over the linear region of the response; the solid circles are the steady-



**Figure 2.** Breath-by-breath  $\dot{V}O_2$  responses as a function of time in a representative subject for (a) incremental-ramp exercise ( $\uparrow$  Ramp;  $30 \text{ W}\cdot\text{min}^{-1}$ ) and (b) maximal decremental-ramp exercise ( $\downarrow$  Ramp;  $30 \text{ W}\cdot\text{min}^{-1}$ ). Asterisk represents  $\theta_L$ . Solid circles represent steady-state responses, with line of best fit (solid line). Lines of best fit to the linear regions of the incremental and decremental ramp responses are shown as dashed lines.

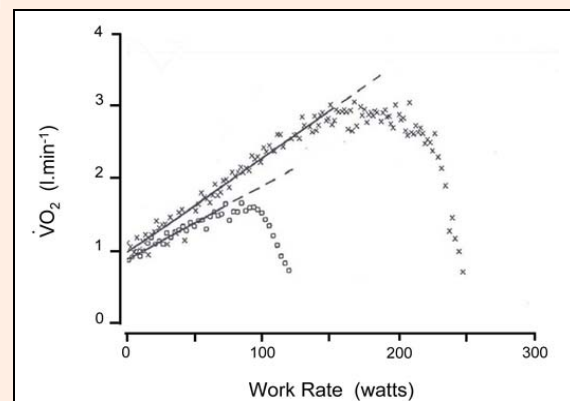
state requirements, determined from the 6-min constant-WR tests. The mean incremental-ramp  $\dot{V}O_2$  slope ( $\Delta\dot{V}O_2/\Delta\text{WR}$ ) was  $10.26 \pm 0.70 \text{ ml}\cdot\text{min}^{-1}\cdot\text{W}^{-1}$  with a range of  $9.0\text{--}11.2 \text{ ml}\cdot\text{min}^{-1}\cdot\text{W}^{-1}$  (Figure 3, solid circles). This response slope was not significantly different from that of the steady-state sub- $\theta_L$   $\dot{V}O_2$  response. However, this 'apparently' first-order  $\dot{V}O_2$  response for the incremental ramp was not evident in the decremental-ramp profile (e.g. Figure 2b). The  $\dot{V}O_2$  slope was appreciably and significantly steeper than that of the incremental-ramp test, i.e.  $\Delta\dot{V}O_2/\Delta\text{WR}$  averaging  $14.16 \pm 1.02 \text{ ml}\cdot\text{min}^{-1}\cdot\text{W}^{-1}$  with a range of  $12.7\text{--}15.5 \text{ ml}\cdot\text{min}^{-1}\cdot\text{W}^{-1}$  (Figure 3, open circles;  $p < 0.005$ ).



**Figure 3.** Individual subject  $\dot{V}O_2$ -WR slope ( $\Delta\dot{V}O_2/\Delta\text{WR}$ ) responses for incremental-ramp exercise (solid circles) and maximal decremental-ramp exercise (open circles); solid and dashed lines, with error bars, represent the respective mean  $\pm$  standard deviation ( $p < 0.005$ ).

To determine whether this was a standard feature for *any* decremental ramp forcing, five of the subjects also performed a submaximal decremental-ramp test such that the peak WR of the decremental ramp was at 90% of  $\theta_L$ . A representative example of the sub- $\theta_L$  decremental ramp

$\dot{V}O_2$  response (open circles), together with the corresponding maximal decremental ramp response (crosses) is presented in Figure 4. In each subject, the  $\dot{V}O_2$  slope (open triangles) (Figure 5) was clearly not as steep as that for the maximal decremental-ramp test (Figure 3, open circles),  $\Delta\dot{V}O_2/\Delta\text{WR}$  averaging  $9.84 \pm 0.90 \text{ ml}\cdot\text{min}^{-1}\cdot\text{W}^{-1}$  and ranging between  $8.2$  and  $10.7 \text{ ml}\cdot\text{min}^{-1}\cdot\text{W}^{-1}$ . This was significantly different from the maximal decremental-ramp  $\Delta\dot{V}O_2/\Delta\text{WR}$  ( $p < 0.005$ ) but not from the incremental ramp value (Figure 5, solid circles).

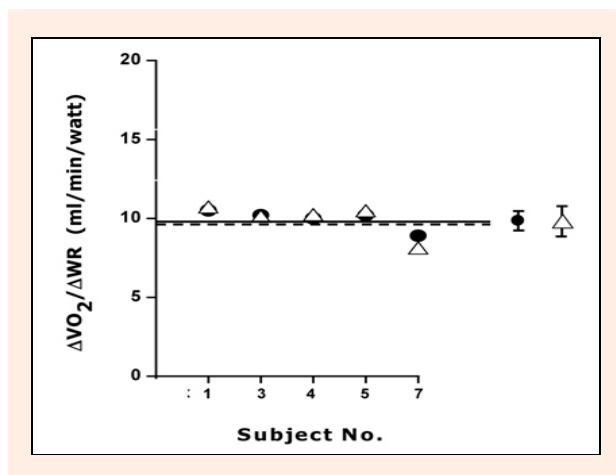


**Figure 4.** Breath-by-breath  $\dot{V}O_2$  responses as a function of work rate, displayed as mirror images, in a representative subject for: maximal decremental-ramp exercise (crosses) and sub-maximal decremental-ramp exercise (open circles). The dashed lines are the lines of best fit over the linear regions of the decremental  $\dot{V}O_2$  response.

## Discussion

The concept of superposition with respect to dynamical systems analysis would suggest that the profile of a first-order dynamic  $\dot{V}O_2$  response to muscular exercise would be predictable, regardless of the dynamic forcing regime employed (e.g. Fujihara et al., 1973; Whipp and Ward,

1981). And so the  $\text{VO}_2$  response to the decremental ramp, performed as a mirror-image of the incremental profile, and importantly over the same time frame, might be expected to yield similar response kinetics. That is, in a dynamically-linear system the  $\text{VO}_2$  response should decrease with the linear profile (after the initial kinetic lag period) equivalent to that expressed by the ramp-incremental test as schematised in Figure 1. It did not, in any of our subjects!



**Figure 5.** Individual subject  $\text{VO}_{2\text{-WR}}$  slope ( $\Delta\text{VO}_2/\Delta\text{WR}$ ) responses for incremental-ramp exercise (solid circles) and sub-maximal decremental-ramp exercise (open triangles); solid and dashed lines, with error bars, represent the respective mean  $\pm$  standard deviation.

However, the  $\text{VO}_2$  response profile to the decremental ramp should, we believe, be considered in the context of the more widely investigated incremental ramp. That is, if, as previously demonstrated (Davis et al., 1982; Hansen et al., 1984; Hughson and Inman, 1986; Whipp et al., 1981), the  $\text{VO}_2$  response to the incremental-ramp tests over the sub- $\theta_L$  region is characteristic of the first-order gain expressed in constant-WR tests over the same intensity range, then the retained linearity over the supra- $\theta_L$  region may also be considered consistent with these first-order features; i.e. the same rate of change of work rate yielding the same rate of change of  $\text{VO}_2$ . Similar to previous studies using ramp-incremental exercise of these durations, there was no evidence in any of the participants in this study (e.g. Figure 2) of an “excess”  $\text{VO}_2$  (or slow component of  $\text{VO}_2$ ). If present, this would be expected to be manifest as a curvilinear increase in the  $\text{VO}_2$  response in the supra- $\theta_L$  region. However, as the slow component of the  $\text{VO}_2$  kinetics has been shown to be both slow and of delayed onset (Barstow and Molé, 1991; Linnarsson, 1974; Paterson and Whipp, 1991; Perrey et al., 2001; although see Stirling and Zakythinaki (2009) for a dissenting viewpoint on the delay characterization), we propose that its influence during rapidly-incremental ramp tests is virtually undetectable; not beginning until a work rate beyond the subject’s  $\theta_L$  and then developing slowly over the remaining, and relatively short, work-rate region. This has also been shown to be the case for constant-WR tests of sufficiently high intensity that the subject reaches the maximum  $\text{VO}_2$  in about 3-4 minutes (e.g. Özyener et al., 2001; Burnley and Jones, 2007).

The inference that the continued linearity of the supra- $\theta_L$   $\text{VO}_2$  response for incremental-ramp exercise reflects first-order behaviour, however, presupposes that the steady-state  $\text{VO}_2$  response in this range likewise remains linear. This is not the case for supra- $\theta_L$  constant-WR exercise, there being a supplemental increase in  $\text{VO}_2$  (i.e.  $\text{VO}_{2\text{sc}}$ ) which increases the  $\text{O}_2$  cost of the exercise above that expected for the wholly-aerobic  $\text{VO}_2$  progression, as demonstrated initially by Whipp and Mahler (1980) and subsequently by others (e.g. Barstow and Molé, 1991; Zoladz et al., 1997; Burnley et al. 2000) – the gain of the fundamental component of the  $\text{VO}_2$  response, however, is either not, or not appreciably, altered (Barstow and Molé, 1991; Jones and Poole 2005; Özyener et al., 2001; Paterson and Whipp 1991). It is of interest, therefore, that very slow WR incrementation rates can result in a  $\text{VO}_2$  response in the supra- $\theta_L$  region that is concave upwards (Hansen et al., 1988; Zoladz et al., 1995, Whipp and Mahler 1980), presumably reflective of the  $\text{VO}_{2\text{sc}}$  having sufficient time to be expressed. Consequently, the  $\text{VO}_2$  response pattern in this supra- $\theta_L$  domain of the incremental-ramp appears to manifest not actual but, what might be termed, pseudo-first-order kinetics.

In contrast, a  $\text{VO}_2$  response consistent with an “excess” component was clearly demonstrable in each of our subjects during the maximal decremental-ramp (e.g. Figures 2 and 5): in general agreement with the work of Yano et al. (2004; 2007). One difference between our findings and those of Yano and colleagues is that we did not see a “breakpoint” in the decremental  $\text{VO}_2$  response at which the  $\text{VO}_2$  slope was reduced at or near the subject’s  $\theta_L$ . In the study of Yano et al. (2004), however, the work-rate decrement began at the same absolute peak work rate, rather than at the individual maxima achieved during the incremental ramp (i.e. a maximal mirror-image symmetry), despite the differences in aerobic fitness of the participants. This difference in methodology between Yano et al. (2004) and the present study, therefore, may have contributed to the differences in the  $\text{VO}_2$  response profile during the decremental-ramp protocol.

The major difference in the metabolic challenge to the maximal decremental work-rate profile, compared to that of the incremental ramp is that: (a) the proportion of type II muscle fibers contributing to the force generation is maximized from exercise onset and then decreases progressively in concert with the work rate – although we are not aware of any studies that have characterised the fiber-type contribution to this kind of exercise, and so our supposition is based on the profiles to increases in work rate; and (b) the anaerobic-glycolytic supplementation to the aerobic component of the energy transfer begins at, or shortly following, the onset of the exercise and with a maximal contribution.

As the lactate production rate is likely to increase to high levels almost immediately, the presence of an “excess”  $\text{VO}_2$  component with the maximal decremental-ramp exercise is, plausibly, consistent with the increased  $\text{O}_2$  cost of metabolizing the lactate. Any lactate that is “cleared” to  $\text{CO}_2$  and  $\text{H}_2\text{O}$  in non-lactate producing fibers will incur only a relatively small, if any, additional  $\text{VO}_2$  cost, i.e. the reduction in glycolytic ATP yield in the fi-

ber(s) (or other tissues) clearing the lactate will be offset by the actual ATP yield in the fibers producing it. The regeneration of depleted glycogen will, of course, have an obligatory and additional  $\text{VO}_2$  cost. However, it is hard to conceive of a significant hepatic component associated with exercise of this duration: repletion presupposes a prior depletion. It also seems unlikely that a muscle fiber that is producing lactate, and hence to some extent depleting its glycogen reserves, will simultaneously reverse the process. However, a fiber that has been producing lactate and then stops contracting in order to reduce the force-generating requirements of the decremental ramp will have the potential to regenerate any glycogen reduction - with its associated increase in  $\text{VO}_2$  cost.

An additional, or alternative, source of the high  $\text{VO}_2$  cost of decremental ramp exercise may arise from an early onset of muscle fatigue consequent to the high degree of muscle requirement (of, presumably, all fibre types) from ramp onset. It has been suggested that muscle fatigue is necessary to generate the  $\text{VO}_{2\text{sc}}$  (Cannon et al., 2011; Poole et al., 1994). Intriguingly, whether the high  $\text{VO}_2$  cost derives from the recruitment of type II muscle fibres (that are less-efficient, and/or have a high  $\text{O}_2$  cost of force production) or from the consequences of fatigue in type I fibres (Cannon et al., 2011; Hepple et al., 2010; Nagesser et al., 1993; Zoladz et al., 2008) remains to be established. The latter may cause an increase in the abundance of type I fibres with cross-bridges in the force-generating state that resist filament sliding (particularly during relaxation), which could result in an increase in the energy (and  $\text{O}_2$ ) cost of force production (Barclay, 1996; and see Jones et al., 2011 for review).

The precise mechanisms contributing to the additional  $\text{VO}_2$  cost in the decremental ramp, therefore, remain to be elucidated. That it is lactate- and/or fatigue-associated, if not lactate-mediated, is supported by the results of Yano et al. (2003; 2004) and of our finding that when the work-rate peak of the decremental ramp was below the subject's  $\dot{V}_{\text{O}_{2L}}$ , the gain of the  $\text{VO}_2$  response was consistent with a first-order response typical of constant work-rate tests in the same intensity domain.

## Conclusion

The mechanisms for the different dynamic  $\text{VO}_2$  response behaviour between incremental and decremental ramps remains to be resolved, with different profiles for fibre type recruitment, muscle fatigue and/or different pathways of lactate clearance being likely to be contributory. Regardless, the  $\text{VO}_2$  response pattern in this supra- $\dot{V}_{\text{O}_{2L}}$  domain of incremental-ramp exercise appears to manifest not actual but what might be termed pseudo-first-order kinetics.

## References

- Barstow, T.J. and Molé, P.A. (1991) Linear and non-linear characteristics of oxygen uptake kinetics during heavy exercise. *Journal of Applied Physiology* **71**, 2099-2106.
- Barclay, C.J. (1996) Mechanical efficiency and fatigue of fast and slow muscles of the mouse. *Journal of Physiology-London* **497**, 781-794.
- Beaver, W.L., Wasserman, K. and Whipp, B.J. (1973) On-line computer analysis and breath-by-breath graphical display of exercise function tests. *Journal of Applied Physiology* **34**, 128-132.
- Beaver, W.L., Lamarra, N. and Wasserman, K. (1981) Breath-by-breath measurement of the true alveolar gas exchange. *Journal of Applied Physiology* **51**, 1662-1675.
- Beaver, W.L., Wasserman, K. and Whipp, B.J. (1986) A new method for detecting anaerobic threshold by gas exchange. *Journal of Applied Physiology* **60**, 2020-2027.
- Burnley, M. and Jones, A.M. (2007) Oxygen uptake kinetics as a determinant of sports performance. *European Journal of Sport Science* **7**, 63-79.
- Burnley, M., Jones, A.M., Carter, H. and Doust, J.H. (2000) Effects of prior heavy exercise on phase II pulmonary oxygen uptake kinetics during heavy exercise. *Journal of Applied Physiology* **89**: 1387-1396.
- Cannon, D.T., White, A.C., Andriano, M.F., Kolkhorst, F.W. and Rositter, H.B. (2011) Skeletal muscle fatigue precedes the slow component of oxygen uptake kinetics during exercise in humans. *Journal of Physiology-London* **589**, 727-739, 2011
- Davis, J.A., Whipp, B.J., Lamarra, N., Huntsman, D.J., Frank, M.H. and Wasserman, K. (1982). Effect of ramp slope on determination of aerobic parameters from the ramp exercise test. *Medicine and Science in Sports and Exercise* **14**, 339-343.
- Fujihara, Y., Hildebrandt, J.R. and Hildebrandt, J. (1973) Cardiorespiratory transients in exercising man. I. Tests of superposition. *Journal of Applied Physiology* **35**, 58-67.
- Hansen, J.E., Casaburi, R., Cooper, D.M. and Wasserman, K. (1988) Oxygen uptake as related to work rate increment during cycle ergometer exercise. *European Journal of Applied Physiology* **57**, 140-145.
- Hansen, J.E., Sue, D.Y. and Wasserman, K. (1984) Predicted values for clinical exercise testing. *American Review of Respiratory Disease* **129** (Suppl), S49-S55.
- Hepple, R.T., Howlett, R.A., Kindig, C.A., Stary, C.M. and Hogan, M.C. (2010) The  $\text{O}_2$  cost of the tension-time integral in isolated single myocytes during fatigue. *American Journal of Physiology-Regulatory Integrative and Comparative Physiology* **298**, R983-R988.
- Hughson, R.L. and Inman, M.D. (1986) Oxygen uptake kinetics from ramp work tests: variability of single test values. *Journal of Applied Physiology* **61**, 373-376.
- Hughson, R.L. and Morrissey, M. (1982) Delayed kinetics of respiratory gas exchange in the transition from prior exercise. *Journal of Applied Physiology* **52**, 921-929.
- Jenkins, J.S., Valcke, C.P. and Ward, D.S. (1989) A programmable system for acquisition and reduction of respiratory physiological data. *Annals of Biomedical Engineering* **17**, 93-108.
- Jones, A.M. and Poole, D.P. (2005) Introduction to oxygen uptake kinetics and historical development of the discipline. In: "*Oxygen Uptake Kinetics in Health and Disease*" Eds: Jones, A.M. and Poole, D. C. London: Routledge Pubs. 3-35.
- Jones, A.M., Grassi, B., Christensen, P.M., Krstrup, P., Bangsbo, J. and Poole, D.C. (2011) The slow component of  $\text{VO}_2$  kinetics: mechanistic bases and practical applications. *Medicine and Science in Sports and Exercise* epub ahead of print.
- Lamarra, N., Whipp, B.J., Ward, S.A. and Wasserman, K. (1987) Effect of interbreath fluctuations on characterizing exercise gas-exchange kinetics. *Journal of Applied Physiology* **62**, 2003-2012, 1987
- Linnarsson, D. (1974) Dynamics of pulmonary gas exchange and heart rate changes at the start and end of exercise *Acta Physiologica Scandinavica* **414** (suppl), 1-68
- Nagesser, A.S., Van Der Laarse, W.J. and Elzinga, G. (1993). ATP formation and ATP hydrolysis during fatiguing, intermittent stimulation of different types of single muscle fibres from *Xenopus laevis*. *Journal of Muscle Research and Cell Motility* **14**, 608-618.
- Neder, J.A., Nery, L.E., Castelo, A., Andreoni, S., Peres, C.A., Sachs, A., Lerario, M.C., Silva, A.C. and Whipp, B.J. (1999) Prediction of metabolic and cardiopulmonary responses to maximum cycle ergometry: a randomized study. *European Respiratory Journal* **14**, 1304-1313.
- Özyener, F., Rossiter, H.B., Ward, S.A. and Whipp, B.J. (2001) Influence of exercise intensity on symmetry of the on- and off-transient kinetics of pulmonary oxygen uptake in humans. *Journal of Physiology-London* **533**, 891-902.
- Paterson, D.H. and Whipp, B.J. (1991) Asymmetries of oxygen uptake

- transients at the on- and off-set of heavy exercise in humans. *Journal of Physiology-London* **443**, 575-586.
- Perrey, S., Betik, A., Candau, R., Rouillon, J.D. and Hughson, R.L. (2001) Comparison of oxygen uptake kinetics during concentric and eccentric cycle exercise. *Journal of Applied Physiology* **91**, 2135-2142.
- Poole, D.C., Barstow, T.J., Gaesser, G.A., Willis, W.T. and Whipp, B.J. (1994)  $\dot{V}O_2$  slow component: physiological and functional significance. *Medicine and Science in Sports and Exercise* **26**, 1354-1358.
- Stirling, J.R. and Zakyntinaki, M. (2009) Counterpoint: the kinetics of oxygen uptake during muscular exercise do not manifest time-delayed phases. *Journal of Applied Physiology* **107**, 1665-1667.
- Whipp, B.J., Davis, J.A., Lamarra, N., Torres, F. and Wasserman, K. (1981) A test to determine parameters of aerobic function during exercise. *Journal of Applied Physiology* **50**, 217-221.
- Whipp, B.J., Mahler, M. (1980) Dynamics of gas exchange during exercise In: *Pulmonary Gas Exchange*, vol. II. Ed: West, J.B. New York: Academic Press. 33-96.
- Whipp, B.J. and Ward, S.A. (1981) Control of ventilatory dynamics during exercise. *International Journal of Sports Med* **1**, 146-159.
- Whipp, B.J., Ward, S.A. and Paterson, D.A. (1992) Dynamic asymmetries of ventilation and pulmonary gas exchange during on- and off-transients of heavy exercise in humans. In: *Control of Breathing and Its Modeling Perspective*. Eds: Honda, Y., Miyamoto, Y., Konno, K. and Widdicombe, J.G. New York: Plenum Press. 237-243.
- Whipp, B.J., Wasserman, K. and Ward, S.A. (1986) Respiratory markers of the anaerobic threshold *Advances in Cardiology* **35**, 47-64
- Yano, T., Yunoki, T. and Ogata, H. (2003) Approximation equation for oxygen uptake kinetics in decrement-load exercise starting from low exercise intensity. *Journal of Physiological Anthropology* **21**, 7-10.
- Yano, T., Yunoki, T., Matsuura, R. and Ogata, H. (2004) Effect of exercise intensity on the slow component of oxygen uptake in decremental work load exercise. *Journal of Physiology and Pharmacology* **55**, 315-324.
- Yano, T., Ogata, H., Matsuura, R., Arimitsu, T. and Yunoki, T. (2007) Comparison of Oxygen uptake at the onset of decrement-load and constant-load exercise. *Physiological Research* **56**, 169-174.
- Zoladz, J.A., Duda, K., Majerczak, J., Domański, J. and Emmerich, J. (1997) Metabolic alkalosis induced by pre-exercise ingestion of  $\text{NaHCO}_3$  does not modulate the slow component of  $\dot{V}O_2$  kinetics in humans. *Journal of Physiology and Pharmacology* **48**, 211-223.
- Zoladz, J.A., Gladden, L.B., Hogan, M.C., Nieckarz, Z. and Grassi, B. (2008) Progressive recruitment of muscle fibers is not necessary for the slow component of  $\dot{V}O_2$  kinetics. *Journal of Applied Physiology* **105**, 575-580.
- Zoladz, J.A., Rademaker, A.C. and Sargeant, A.J. (1995) Non-linear relationship between  $\text{O}_2$  uptake and power output at high intensities of exercise in humans. *Journal of Physiology-London* **488**, 211-217.

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### Key points

- The slope of the decremental-ramp response is appreciably greater than that of the incremental.
- The response dynamics in supra- $\theta_L$  domain of the incremental-ramp appear not manifest actual first-order kinetics.
- The mechanisms underlying the different dynamic response behaviour for incremental and decremental ramps are presently unclear.